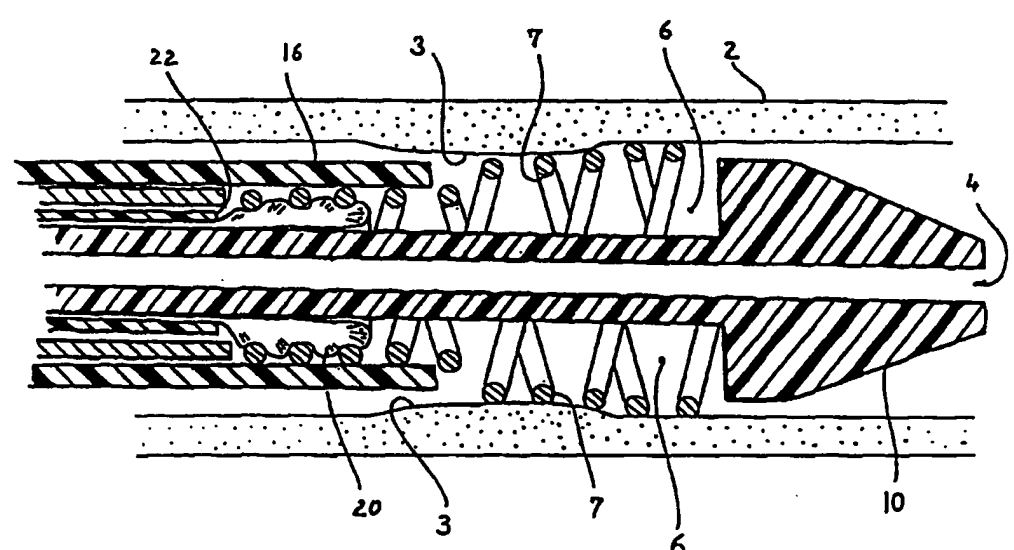




## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

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<p>(54) Title: REVERSIBLE-ACTION ENDOPROSTHESIS DELIVERY DEVICE</p>  <p>(57) Abstract</p> <p>A reversible-action endoprosthesis delivery device (1) comprising an axially extending inner tube (8) surrounded by an outer sheath (16) comprising remotely activable retaining means (20) for maintaining or releasing the endoprosthesis (7) in a fixed axial relationship relative to the inner tube (8) so that up to the end of the placement procedure, the endoprosthesis (7) can be withdrawn and replaced in a more suitable position.</p>		

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Reversible-action endoprosthesis delivery device.

DESCRIPTION :

The invention concerns devices for the placement of luminal endoprostheses in animal, including human body  
5 vessels.

In particular, it relates to such a device for the deployment and retraction of a stent, particularly a self-expanding stent.

Advance in angioplasty now results in a  
10 particular attention to be given to the precise positioning of endoprosthesis in vessels to be cured. This is particularly true for small vessels.

BACKGROUND OF THE INVENTION :

Several attempts have already been made to  
15 achieve the possibility of controlling the position of a stent in a delivery device during the placement operation, before its full length becomes radially expanded.

US 5,026,377 discloses a stent delivery device for a self-expanding stent such as the one disclosed in  
20 US-A-4,665,771. The proximal end of the stent to be released is fastened to a central pusher of the device either by an adhesive, or by a local widening of this pusher.

WO 96/13228 discloses a stent delivery device  
25 provided with a soft "recapture sleeve" - generally bearing crossed grooves - located on the central pusher of the device in order to prevent axial displacement of a self-expanding stent relative to the pusher before a given fraction of the length of the stent has been allowed to  
30 expand.

In practice, however, these devices do not provide fully reliable results.

Just before its deployment in the vessel, the  
35 stent is located inside a chamber toward the distal end of

the delivery device. Once the stent has been partially deployed and hence allowed to expand, it places itself against the interior wall of the vessel. It proves difficult to force it back into the chamber. Indeed, 5 instead of entering back the chamber, the stent is often ripped out of the end of the delivery device and thus can no longer be displaced without being destroyed or removed by surgery.

Furthermore, the recapture means of the devices 10 according to the state of the art add to the radial cumbersomeness of the delivery device.

There has therefore been a strong need for a space-saving and efficient reversible-action endoprosthesis delivery device.

15 BRIEF SUMMARY OF THE INVENTION :

A precise positioning of the stent requires a precise control of its position via the pusher, whatever the solicitations the stent is subjected to.

To this end the invention provides a 20 reversible-action endoprosthesis delivery device extending between a distal end and a proximal handling end, comprising an axially extending inner tube surrounded by an outer sheath, the inner tube comprising, near its distal end, a chamber able to enclose an expendable endoprosthesis 25 in a radially contracted state, the inner tube being axially movable relative to the outer sheath. The delivery device of the invention is characterised in that it comprises remotely activable retaining means for selectively maintaining the endoprosthesis in a given axial 30 relationship in relation to the inner tube and releasing same. Remotely activable retaining means have now been developed, allowing the possibility of entering vessels of small diameter, a strong retaining effect being produced at will when the proximal end of the delivery device carrying 35 the stent has been driven up to the place to be cured. Because the means are remotely activable the retaining

force can be applied when needed and at the position where such force is needed, making it possible to re-position the stent without damaging the vessel walls.

5           According to a preferred embodiment, the remotely activable retaining means comprises an inflatable balloon fixed to the inner tube, this balloon being connectable to pressure means placed at the proximal end of the delivery device. Thereby a simple, and not cumbersome,  
10 yet reliable remotely activable retaining means is provided. Furthermore the strength of the retaining force can accurately be controlled and regulated by means of the pressure in the balloon.

          The inflatable balloon is preferably placed near  
15 the proximal part of the chamber.

          The balloon is advantageously able to be inflated up to a diameter corresponding to the diameter of a body vessel.

          Preferably, the device is able to enclose a  
20 self-expanding endoprosthesis and particularly an endoprosthesis made of a braid of shape-memory alloy.

          The endoprosthesis can also comprise a balloon-expandable stent.

          The outer sheath is preferably reinforced by a  
25 multiwire braiding, advantageously of metal wires.

#### Brief description of the drawings

          Other advantages of the invention will become apparent when referring to the description hereafter of several embodiments, given as non-limiting examples,  
30 reference being made to the appended drawings wherein

          Fig. 1 is a diagrammatic view of a cross-section of the distal part of one embodiment of a device according to the invention.

          Fig. 2 is a diagrammatic view of the device of  
35 Fig. 1 at an early stage of the deployment operation.

          Fig. 3 is a diagrammatic view of the device of

Figs. 1, 2 at a later stage of the deployment operation.

Fig. 4 is a diagrammatic view of a possible use of a device according to Fig. 1 after complete release of a stent.

5            Fig. 5 is a diagrammatic view of another embodiment of the device at a stage corresponding to Fig. 3.

Fig. 6 is a diagrammatic view of still another embodiment at the same stage of deployment.

10 DETAILED DESCRIPTION OF THE SEVERAL VIEWS :

On Fig. 1, a delivery device 1 according to the invention has been introduced, according to a known procedure, up to a lesion 2 to be cured in a body vessel 3, in the present case a stenosis in an artery 3.

15            The distal end 4 of the device comprises a chamber 6 wherein an expandable endoprosthesis - represented here as a self-expanding stent 7 - has been inserted in a radially contracted state.

20            The chamber 6 extends around an inner tube 8, between an atraumatic tip 10 and a stent pusher 12. An axial lumen 14 allows the whole delivery device 1 to be driven along a guide wire (not shown).

25            The chamber 6 is closed by an outer sheath 16 which is axially movable at will relative to the inner tube 8.

30            The optimal position of the stent 7 after release and expansion can be carefully checked before starting the release process thanks to the presence of radio-transparent markers 18 embedded in the otherwise radio-opaque outer sheath 16.

35            The delivery device 1 according to the invention also comprises a remote controlled retaining device, that in the present embodiment comprises an inflatable micro-balloon 20 connected to pressure means (not represented) placed at the proximal end of the delivery device 1.

During the insertion steps, the micro-balloon 20 remains in a deflated state, this having virtually no influence on the diameter of the device 1, which can be inserted into very thin vessels 3.

5           The supposedly optimal position of the device for the deployment of the stent being determined, the micro-balloon 20 is slightly inflated, causing the proximal end of the stent 7 to be firmly locked in place with respect to the inner tube 8.

10           The outer sheath 16 can now be moved backwards, as represented on Fig. 2, uncovering the distal end of the stent 7 which expands radially either because of its own resilience, or due to the change of temperature it undergoes in case the stent is made of a material  
15 undergoing a phase transition at body temperature.

This stage is critical for most of the delivery devices of the known art which are supposed to have the possibility of forcing back the stent into its chamber.

20           Indeed, as soon as the stent is deployed, it becomes anchored to the inner wall of vessel and it thus exerts on the outer sheath of the device a resistance sufficient to cause its proximal end to be ripped out of the still closed proximal part of the chamber 6.

25           This effect is dramatically increased when the stent is a self-expanding stent, in particular when it is made out of a material undergoing a phase transition (e.g. Nitinol) at body temperature.

With classical delivery devices, the operator  
30 does not have the possibility to step backwards when he realizes that, for some reason, the stent is not perfectly at its right place.

On the contrary, remote-activated retaining means 20 that are part of the device 1 according to the  
35 invention provides for a very firm grasp on the stent 7, allowing the inner tube 8 to be slid back relative to the

outer sheath 16 up to the initial (closed) position of the chamber 6, even when the stent 7 has been previously deployed up to 80% of its length.

Thanks to the retaining means 20, it has become possible to re-position the stent 7 in a more adequate position, either after an axial displacement, or after a rotation as the case may be.

When the stent 7 has been given its correct position, the retaining device 20 can be deflated and the outer sheath 16 is pulled fully backwards, as represented on Fig. 3.

The device 1 of the invention can then be removed through the expanded stent 7 or, as can be seen from Fig. 4, it can provide for a further advantageous step.

If the control screen reveals that the operation has not been absolutely successful (e.g., as shown on Fig. 3, when the stenosis 2 prevents the stent 7 from fully expanding), it remains possible, without removing the device 1, to further use the retaining micro-balloon 20, acting now, as a classical dilatation balloon, by moving the entire device 1 forwards and inflating the micro-balloon 20 again, this time at a pressure sufficient for it to reach the diameter of the vessel 2 to be cured. The use of the present device 1 thus allows a precious gain on the time spent for the operation and on the pain the patient has to endure.

The pressure required to inflate the micro-balloon 20 is exerted by a fluid carried along a second lumen 22 extending along the axial lumen 4 of the inner tube 8.

This inner tube 8 is preferably rigid, so as to avoid kinking during the introduction steps. PEEK (polyether ketone) or POM (polyacetol) are, inter alia, particularly suitable materials.

The inflatable balloon 20 must also be made of a



rigid and not compliant material, but it can also be compliant so as to comply with the shape of the stent 7. It can be made out of PE or PET (Polyethylene or polyethylene terephthalate).

5           The external diameter and the length of the balloon 20 must be carefully chosen so as to avoid an excessive inflation at its distal end, which could lead to refraining the stent 7 from being driven back into the chamber 6.

10           The outer sheath 16 must of course afford an excellent resistance to compression in order not to become distended by the stent 7. The outer sheath 16 is preferably reinforced by a multiwire braiding 24 as shown in Fig. 5 and 6.

15           Here again, POM or PEEK or other organic materials are best suitable.

          The driving fluid can be fed by a known inflation syringe connected to the second lumen 22 via a known Y-adapter (not shown).

20           Figs. 5 and 6 display two possible embodiments of the second lumen 22 and of the balloon 20. As can be seen on Fig. 5, the balloon 20 is fixed at its distal end to the inner tube 8 and, at its proximal end, of the peripheral side of the pusher 12, the second lumen  
25 extending between the inner tube 8 and the pusher 12.

          Fig. 6 displays an embodiment wherein the inner tube 8 encloses two separated lumens. A first lumen 14 for passing the guide wire 26 is continued through the atraumatic tip 10. A second lumen 22 comprises at least one  
30 lateral outlet 28 communicating with the inner volume of the micro-balloon 20. This second lumen 22 is blocked up at its distal end, toward the atraumatic tip 10.

          In short, the invention can be described as follows :

35           A reversible-action endoprosthesis delivery device (1) comprising an axially extending inner tube (8)

surrounded by an outer sheath (16) comprising remotely activable retaining means (20) for maintaining or releasing the endoprosthesis (7) in a fixed axial relationship relative to the inner tube (8) so that up to the end of the  
5 placement procedure, the endoprosthesis (7) can be withdrawn and replaced in a more suitable position.

## C L A I M S

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1.- A reversible-action endoprosthesis delivery  
5 device (1) extending between a distal end (4) and a  
proximal handling end, comprising an axially extending  
inner tube (8) surrounded by an outer sheath (16), the  
inner tube (8) comprising, near its distal end, a chamber  
(6) able to enclose an expendable endoprosthesis (7) in a  
10 radially contracted state, the inner tube (8) being axially  
movable relative to the outer sheath (16), characterised in  
that the delivery device comprises remotely activable  
retaining means (20) for selectively maintaining or  
releasing the endoprosthesis (7) in a given axial  
15 relationship relative to the inner tube (8) and to release  
same.

2.- A delivery device (1) according to claim 1  
characterised in that the remotely activable retaining  
means (20) comprises an inflatable balloon (20) fixed to  
20 the inner tube (8), this balloon (20) being connectable to  
pressure means placed at the proximal end of the delivery  
device (1).

3.- A delivery device according to claim 2  
characterised in that the inflatable balloon (20) is placed  
25 near the proximal part of the chamber (6).

4.- A delivery device according to claim 2 or 3,  
characterised in that the balloon (20) is able to be  
inflated up to a diameter corresponding to the diameter of  
a body vessel (2).

30 5.- A delivery device (1) according to claim 1  
to 5, characterised in that the outer sheath (16) is  
reinforced by a multiwire braiding.

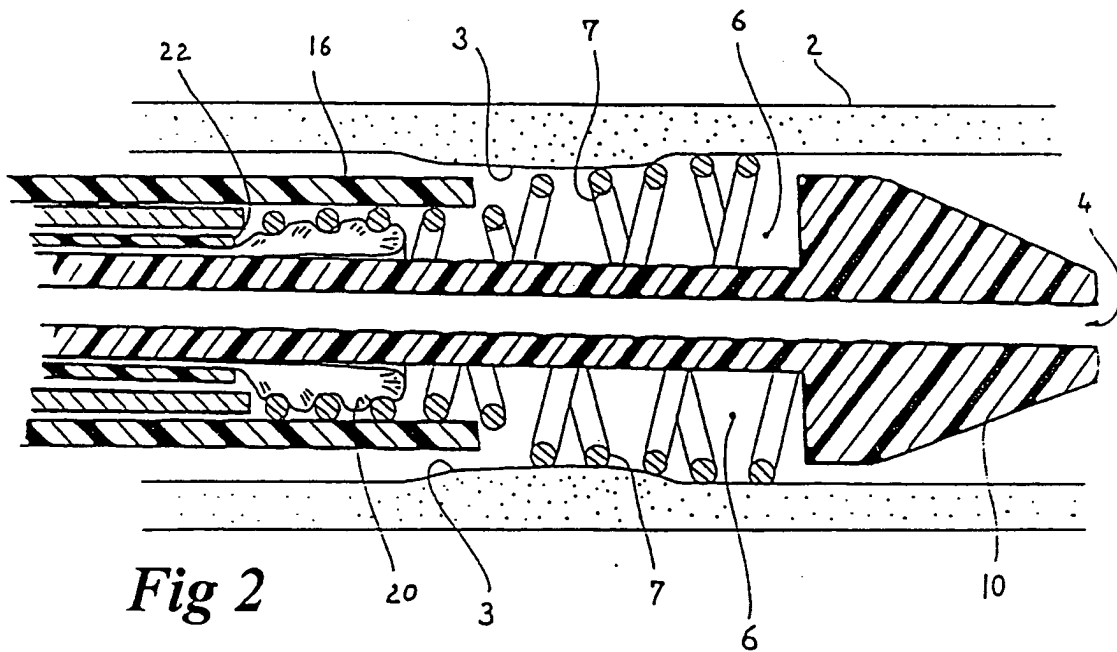
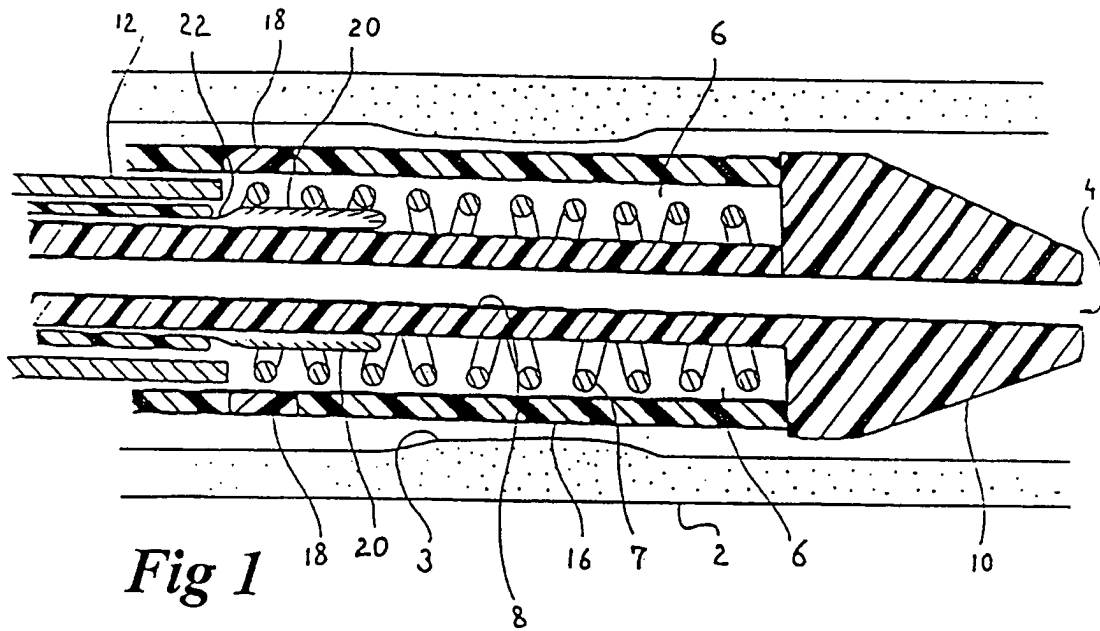
6.- A delivery device according to claim 5  
characterised in that the braiding is made of metal wires.

35 7.- A delivery device according to claim 1 to 6  
characterised in that it is able to enclose a self-

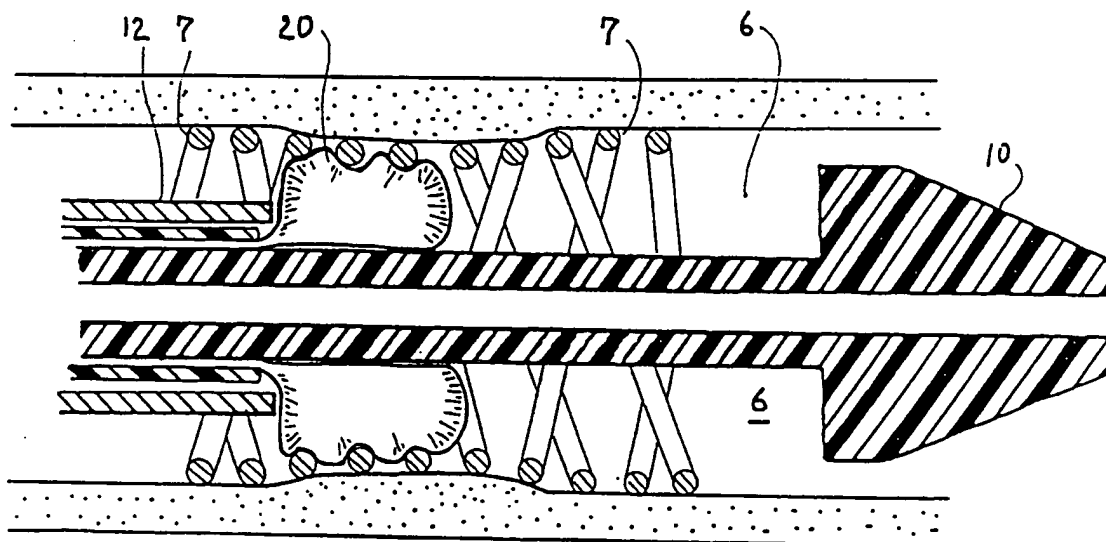
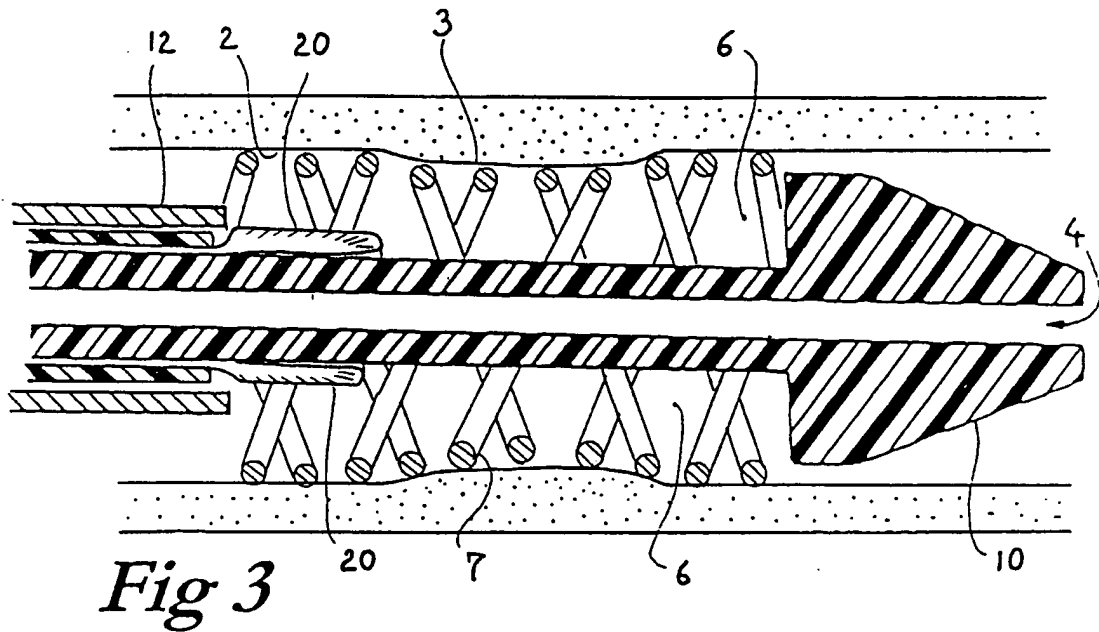
expandable endoprosthesis (7).

8.- A delivery device according to claim 7, characterised in that it comprises a self-expandable endoprosthesis made of a braid of shape-memory alloy.

5 9.- A delivery device according to claim 1 to 8, characterised in that it comprises an endoprosthesis (7) with a balloon expendable stent.

$\frac{1}{3}$ 

2/3

*Fig 4*



# INTERNATIONAL SEARCH REPORT

International Application No

PCT/IB 99/00446

**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC 6 A61F2/06

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61F

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO 97 17899 A (CORVITA CORP.) 22 May 1997 see abstract see page 4, line 4 - line 17 see page 5, paragraph 4 - page 6, paragraph 2; figures 4-12 ---	1-9
A	US 5 695 499 A (HELGERSON ET AL.) 9 December 1997 see abstract see column 1, line 63 - line 65 see column 2, line 14 - line 36; figures 1,2,4,6-8 ---	1-9
A	WO 97 17914 A (SCIMED LIFE SYSTEMS, INC.) 22 May 1997 see abstract see page 3, line 14 - page 5, line 13; figures 1,2,4,5,11 ---	1-9
	-/--	

☒ Further documents are listed in the continuation of box C.

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Date of the actual completion of the international search

9 June 1999

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17/06/1999

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European Patent Office, P.B. 5818 Patentlaan 2  
NL - 2280 HV Rijswijk  
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,  
Fax: (+31-70) 340-3016

Authorized officer

Michels, N



# INTERNATIONAL SEARCH REPORT

Int. Application No.  
PCT/IB 99/00446

## C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	EP 0 705 576 A (CORDIS EUROPA N.V.) 10 April 1996 -----	

# INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

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